

This article was downloaded by:

On: 22 January 2011

Access details: *Access Details: Free Access*

Publisher *Taylor & Francis*

Informa Ltd Registered in England and Wales Registered Number: 1072954 Registered office: Mortimer House, 37-41 Mortimer Street, London W1T 3JH, UK



The Journal of Adhesion

Publication details, including instructions for authors and subscription information:

<http://www.informaworld.com/smpp/title~content=t713453635>

In-situ Measurement of the Properties of Curing Systems with Microdielectrometry

S. D. Senturia^a; N. F. Sheppard Jr.^a; H. L. Lee^a; D. R. Day^a

^a Department of Electrical Engineering and Computer Science, and Center for Materials Science and Engineering, Massachusetts Institute of Technology, Cambridge, MA, U.S.A.

To cite this Article Senturia, S. D. , Sheppard Jr., N. F. , Lee, H. L. and Day, D. R.(1982) '*In-situ* Measurement of the Properties of Curing Systems with Microdielectrometry', The Journal of Adhesion, 15: 1, 69 – 90

To link to this Article: DOI: 10.1080/00218468208073217

URL: <http://dx.doi.org/10.1080/00218468208073217>

PLEASE SCROLL DOWN FOR ARTICLE

Full terms and conditions of use: <http://www.informaworld.com/terms-and-conditions-of-access.pdf>

This article may be used for research, teaching and private study purposes. Any substantial or systematic reproduction, re-distribution, re-selling, loan or sub-licensing, systematic supply or distribution in any form to anyone is expressly forbidden.

The publisher does not give any warranty express or implied or make any representation that the contents will be complete or accurate or up to date. The accuracy of any instructions, formulae and drug doses should be independently verified with primary sources. The publisher shall not be liable for any loss, actions, claims, proceedings, demand or costs or damages whatsoever or howsoever caused arising directly or indirectly in connection with or arising out of the use of this material.

In-situ Measurement of the Properties of Curing Systems with Microdielectrometry

S. D. SENTURIA, N. F. SHEPPARD, Jr., H. L. LEE and D. R. DAY

Department of Electrical Engineering and Computer Science, and Center for Materials Science and Engineering, Massachusetts Institute of Technology, Cambridge MA 02139, U.S.A.

(Received February 24, 1982; in final form May 5, 1982)

This paper addresses the *in-situ* measurement of various properties of curing systems with a particular dielectric method called Microdielectrometry. We have used integrated circuit technology to develop a miniaturized dielectric probe that combines small size with built-in amplification to achieve sensitivity at frequencies as low as 1 Hz. The device combines a planar interdigitated electrode structure with a pair of matched field-effect transistors. Calibration is based entirely on the details of the electrode geometry, and thus is stable with respect to temperature variations, and is reproducible from device to device. Generally, what is measured is the frequency dependent dielectric permittivity (ϵ') and dielectric loss factor (ϵ'') in the frequency range 1–1000 Hz. In this paper, the results of isothermal cures of the amine-epoxy system DGEBA-MPDA are presented, and are shown to provide a measurement of a low-frequency dielectric relaxation time which can be correlated with bulk viscosity prior to gelation. We also present a study of the effects of PGE diluent on the DGEBA-DDS system, both during isothermal cures at 140°C, and in post-cure ramped temperature studies. It is shown that as little as 5% diluent produces observable changes in the low-frequency dielectric properties, and that frequencies below 10 Hz are more sensitive than higher frequencies to the effects of diluent on the dominant low-frequency dielectric relaxation associated with the glass transition.

INTRODUCTION

As new materials and cure methods are developed, the ability to make direct measurements of the properties of curing systems is central both to the analysis of the effects of a modified material or cure method, and to the evaluation of the resulting materials for practical applications. Mechanical and rheological

Presented at the Annual Meeting of The Adhesion Society, Mobile, Alabama, U.S.A., February 21–24, 1982.

methods address macroscopic properties, while spectroscopic methods address properties on a microscopic molecular level. Dielectric methods share both macroscopic and microscopic features, in that the dipoles being oriented during dielectric measurements are of microscopic origin, whereas the degree and speed of their orientation may depend on macroscopic properties of the curing system, such as viscosity and the tightness of the cross-linked network.

This paper addresses the *in-situ* measurement of various properties of curing systems with a particular dielectric method called Microdielectrometry.^{1,2,3} We have used integrated circuit technology to develop a miniaturized dielectric probe that combines small size with built-in amplification to achieve sensitivity at frequencies as low as 1 Hz. The device combines a planar interdigitated electrode structure with a pair of matched field-effect transistors. Calibration is based entirely on the details of the electrode geometry, and thus is stable with respect to temperature variations, and is reproducible from device to device. The Microdielectrometer “chip” can be implanted in a bulk specimen, or it can be used by placing a few milligrams of sample on the active device region. With suitable packaging, the device can be used in a wide range of environments, and can function at temperatures up to 250°C.

We have used Microdielectrometry to follow the changing low frequency dielectric properties of a variety of curing systems, including amine cured epoxies, polyimides, phenolics, and various rubbers. Generally, what we measure is the frequency dependent dielectric permittivity (ϵ') and dielectric loss factor (ϵ'') in the frequency range 1–1000 Hz. In the specific cases to be discussed in this paper, these dielectric properties are interpreted in terms of more fundamental properties of the system, such as viscosity, and the structure of the cross-linked network.

We have studied isothermal cures of diglycidyl ether of bisphenol A (DGEBA) with *m*-phenylene diamine (MPDA) at temperatures in the range 60–100°C. The variation of ϵ' and ϵ'' with frequency at any instant of cure prior to gelation can be used to determine a low-frequency dielectric relaxation time, τ , which can be correlated with the bulk viscosity. We have also examined the effect of the diluent phenyl glycidyl ether (PGE) on DGEBA cured with diaminodiphenylsulfone (DDS), both during cure at 140°C and in post-cure ramped temperature studies. It is found that as little as 5% diluent produces observable changes in the low-frequency dielectric properties, and that frequencies below 10 Hz are more sensitive than higher frequencies to the effects of the dominant low-frequency dielectric relaxation associated with the glass transition.

EXPERIMENTAL

A. Microdielectrometry

The usual method for making measurements of dielectric properties is to place the sample between closely spaced parallel conducting plates, and to monitor the AC equivalent capacitance and dissipation factor of the resulting capacitor. The capacitance is proportional to the dielectric permittivity (ϵ') at the measurement frequency, and the dissipation factor in combination with the ϵ' value can be used to extract the dielectric loss factor (ϵ''). The calibration of the measurement depends on the area of the plates and on their spacing. When used for *in-situ* measurements in curing systems, plate spacing can change with either temperature or stress, with the result that the calibration for ϵ' and ϵ'' can be affected. However, since both calibrations are affected equally by geometry changes, their ratio, the loss tangent ($=\epsilon''/\epsilon'$), is not affected. Hence, when making conventional measurements, one often monitors loss tangent rather than ϵ' or ϵ'' during cure.

The approach taken in Microdielectrometry is fundamentally different. Instead of using a parallel plate geometry, both electrodes used in the dielectric measurement are placed on the same surface of an integrated circuit (see Figure 1 for a schematic top view), and the medium to be studied is placed over the electrodes, either by application of a small sample or by embedding the entire integrated circuit in the curing medium (see Figure 2 for a schematic cross section through the electrode region). Because this electrode geometry is less efficient than parallel plates in terms of coupling the electric field through the sample medium, amplification is required in the form of a field-effect transistor whose gate electrode is one of the two interdigitated electrodes (called the floating gate; see Fig. 1). To compensate for the transistor amplification factor, which would require a complex calibration procedure at each operating temperature, a second identical field-effect transistor is simultaneously fabricated on the same integrated circuit (see Figure 3 for a microphotograph of the device). The second field-effect transistor serves as a reference in a differential feedback circuit, the details of which have been published elsewhere.⁴ The net effect of the two-transistor plus feedback circuit combination is that when a sinusoidal signal is applied to the driven electrode, the corresponding sinusoidally varying voltage that appears on the floating gate can be measured independent of transistor amplification factor. This floating-gate voltage has an amplitude and phase relative to the drive signal that depends on the geometry of the device and on the dielectric properties of the sample medium. The device geometry is both stable and reproducible. Thus, the task of calibrating the measurement reduces to relating the measured amplitude and phase for a particular device geometry to the specific values of ϵ' and ϵ'' for the sample.

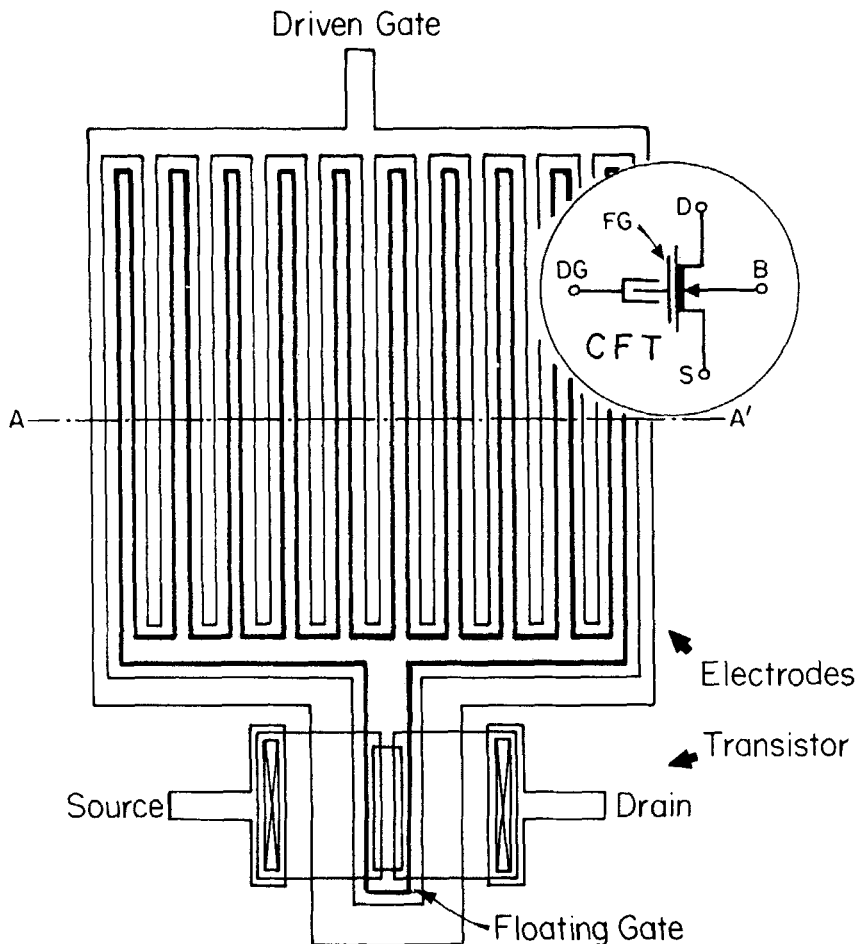


FIGURE 1 Schematic view of active portion of Microdielectrometer chip. CFT refers to "floating-gate charge-flow transistor", of which the Microdielectrometer is an example.

We have developed a computerized instrumentation system for use in Microdielectrometry (see Figure 4). A Hewlett-Packard HP85 calculator serves as controller and data-logger. Archival data storage is done on tape cassettes. Provision is made for making programmed measurements at many different frequencies, and for monitoring temperature during the experiment. The calibration of the basic amplitude-phase data in terms of ϵ' and ϵ'' (see below) is stored in the calculator memory as a lookup table that is used in conjunction with an interpolation program. The system also has provision for operating a

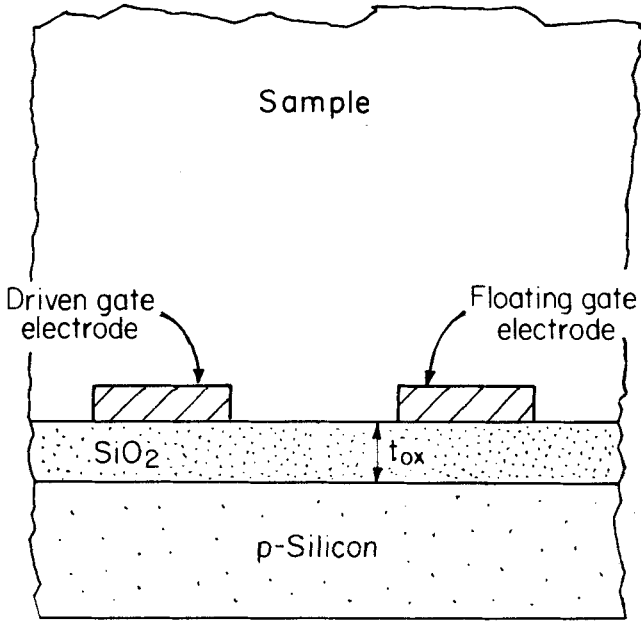


FIGURE 2 Schematic cross-section through electrode region.

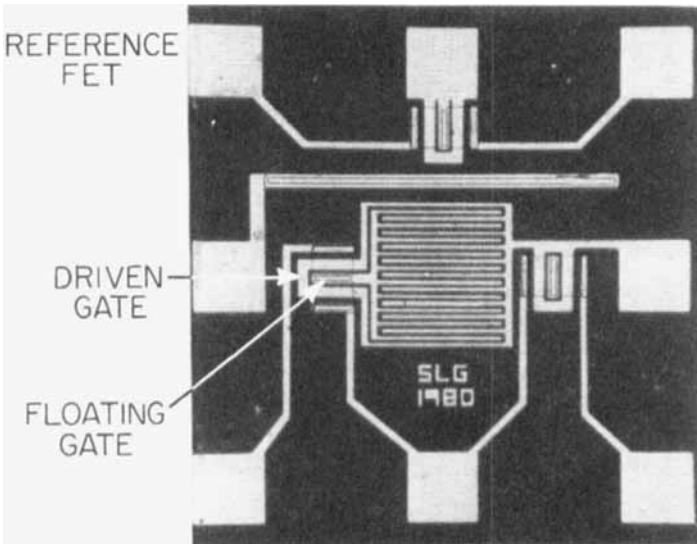


FIGURE 3 Photomicrograph of chip. Dimensions are 75×75 mils.

MEASUREMENT SYSTEM

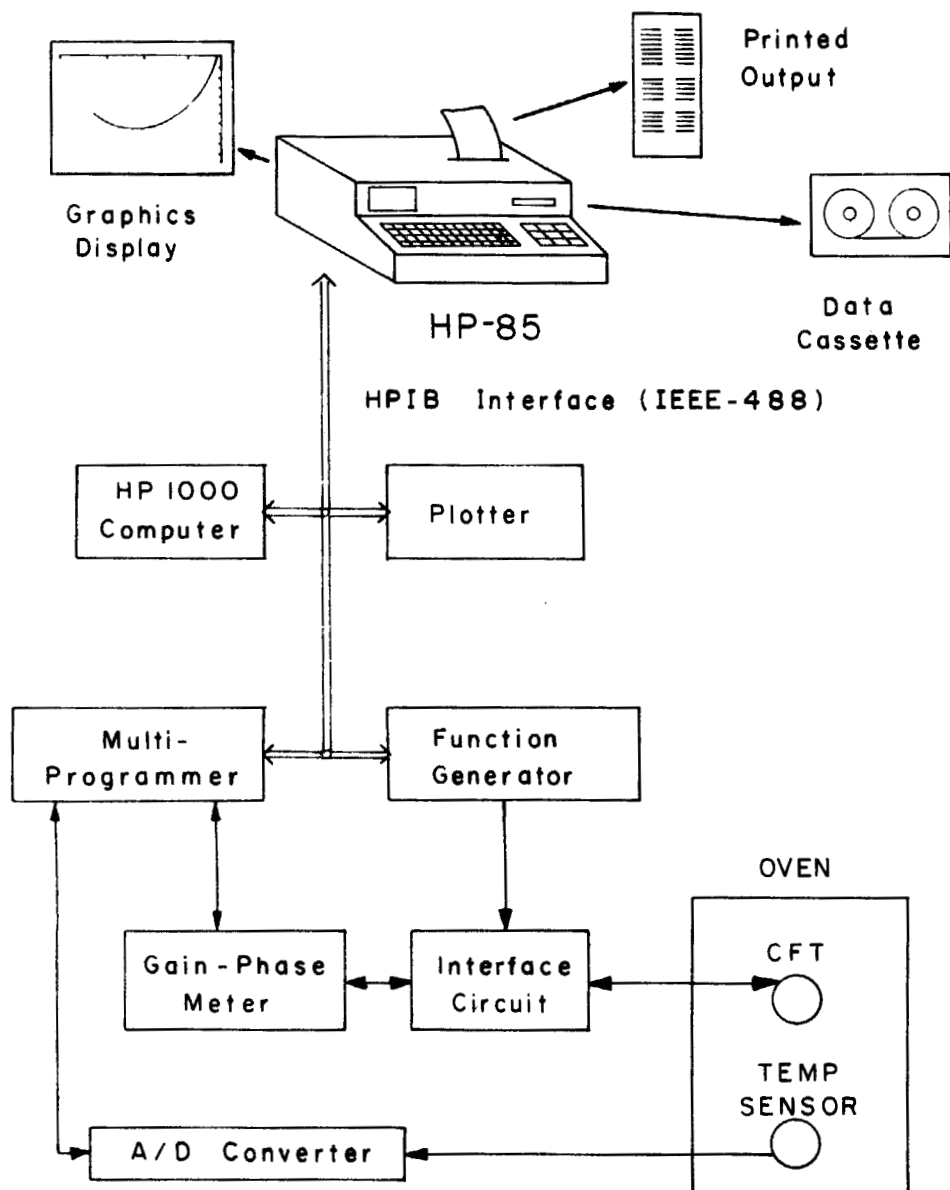


FIGURE 4 Block diagram of Microdielectrometry instrumentation.

line printer and a graphics plotter, and data files can be transferred to other computers such as our laboratory's HP-1000 if large-scale computations are required.

B. Calibration

The fact that the sensing electrode is electrically floating, combined with the proximity of the amplifier to that electrode, means that good signal-to-noise ratio can be achieved at very low frequencies. However, the electrode geometry is more difficult to calibrate than conventional parallel plates. We have approached the calibration problem by setting up a computer solution to the two-dimensional Laplace equation for our device geometry assuming that the material is both isotropic and homogeneous.⁵ This approach ignores surface and electrode effects, but permits a calculated calibration to be obtained for all ranges of ϵ' and ϵ'' . Figure 5 shows a typical set of calibration curves. Each measurement yields an amplitude (gain in decibels) and a phase (in degrees). Contours of constant ϵ' and ϵ'' are plotted in this gain-phase space, permitting the interpretation of measured data in terms of dielectric properties.

Experimental verification (and/or modification) of the calculated calibration is made difficult by the intrinsic problem of preparing calibration materials with known dielectric permittivity and loss factor. Along the gain axis, however, which corresponds to low loss factor, the contours of constant ϵ'' bunch together. Therefore, for low-loss materials, there is a direct correspondence between ϵ' and gain. We have verified the calculated ϵ' values along this axis with various low-loss dielectric fluids and with the bare device in air ($\epsilon' = 1.0$), and find agreement to better than 10%. However, at low values of ϵ'' , any errors in phase measurement will limit the precision of the ϵ'' determination. For our present device design, packaging, cabling arrangement, and choice of phase-measurement instrument (HP 3575A), phase measurements corresponding to ϵ'' values below about 0.02 cannot be reliably interpreted. There is nothing fundamental about this limitation; it represents the present state of our progress with the calibration.

There is another difficult portion of the gain-phase space, corresponding to high-loss factors, where the contours of constant ϵ' bunch together. In this region, accurate determination of ϵ' is difficult. Furthermore, any small measurement errors, either in gain or phase, can produce errors in both ϵ' and ϵ'' in this high-loss region. Our present capabilities allow measurement of ϵ'' up to about 100, and measurement of ϵ' wherever ϵ'' is less than about 30. Outside these limits, the calibration is not valid at present.

In the central region of the gain-phase space, where contours are well spaced, there is adequate sensitivity to determine both ϵ' and ϵ'' to within a few percent. However, the absolute accuracy of the calibration in this region has

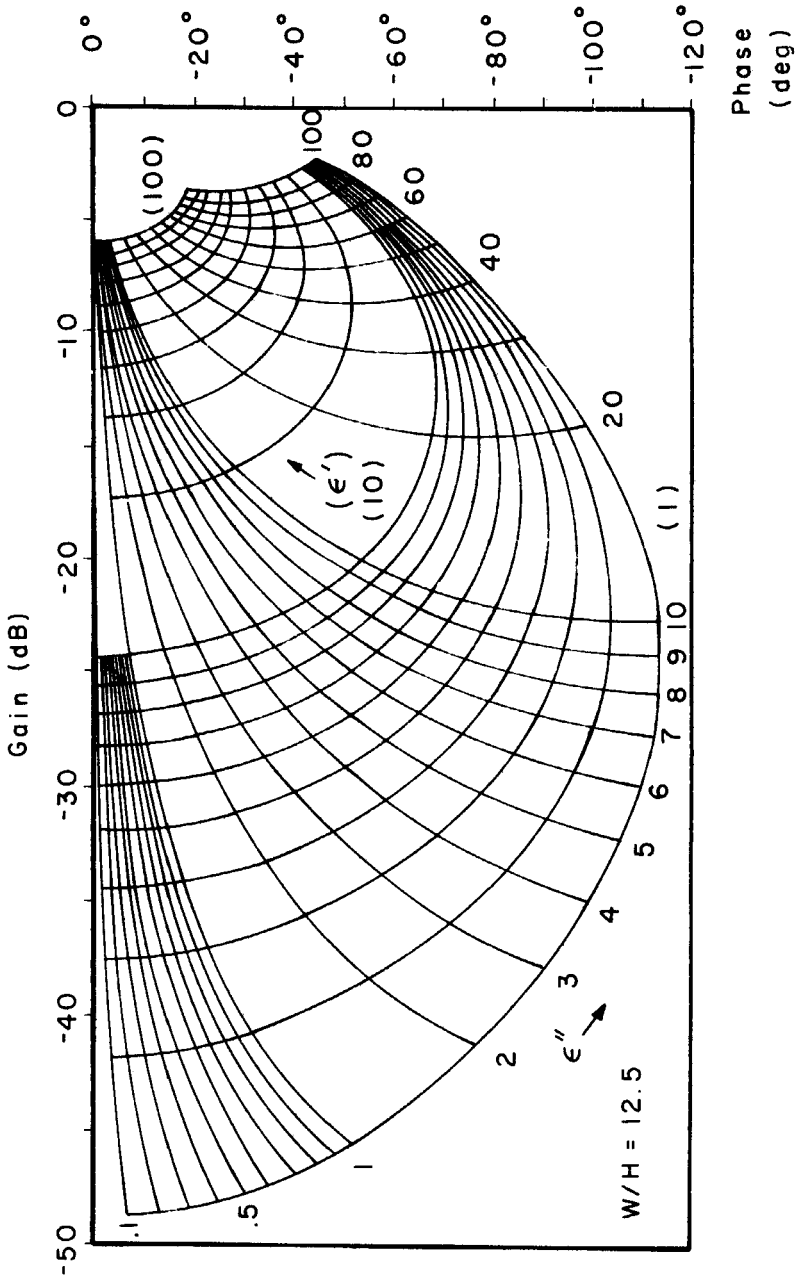


FIGURE 5 Calculated calibration curves for the Microdielectrometer chip.

not yet been established. Comparison measurements made on nominally identical samples using devices with different geometries are being done to explore this issue.

C. Samples and measurements

The materials used in this study were a bifunctional epoxy, diglycidyl ether of bisphenol A (DGEBA), having an epoxide equivalent weight of 175; a reactive epoxide diluent, phenyl glycidyl ether (PGE); and two amine curing agents, *m*-phenylene diamine (MPDA), and diaminodiphenyl sulfone (DDS). All epoxy-amine samples were prepared in 2–3-g batches using a stoichiometric amount of epoxide and amine functionalities. The components were weighed out, melted together over low heat until dissolved, cooled, and stored in a refrigerator until use, for at most a period of a week.

Microdielectrometer chips having aluminum electrodes with a between electrode spacing of 12 microns and having electrode-to-substrate spacings of both 1000 nm and 540 nm were fabricated using standard MOS technology in the MIT Microelectronics Laboratory.⁴ The individual chips were attached to TO-99 transistor headers, and leads were attached using ultrasonically bonded 1 mil aluminum wire. The resin samples were applied to the electrode area by first heating the resin slightly until it flowed, then applying a few drops with an eyedropper. The experiments were performed in the oven of a modified gas chromatograph, which permitted isothermal or programmed ramp temperature cycles.

RESULTS AND DISCUSSION

A. DGEBA-MPDA

Typical results⁶ for the time dependence of ϵ' and ϵ'' for the DGEBA-MPDA system at 60 and 100°C are shown in Figures 6 and 7. Data are presented for three frequencies (a total of seven were measured), and for devices with electrode-to-substrate spacing of 1000 nm (devices with 540 nm spacing were also used). Times to gelation t_g for this resin system are also shown for reference.⁷ Comparison between Figures 6 and 7 shows that the behavior of the dielectric properties is similar, but occurs over a longer time scale as the temperature is decreased.

An obvious result from the data is that both ϵ' and ϵ'' are strongly dispersive (*i.e.*, frequency dependent). Hindered dipole rotation and hindered bulk conduction (presumed ionic) can each lead to such dispersion. The ideal Debye model for hindered rotation is illustrated in Figure 8. When the product $\omega\tau$ is small (ω is the angular frequency, τ the dielectric relaxation time), the

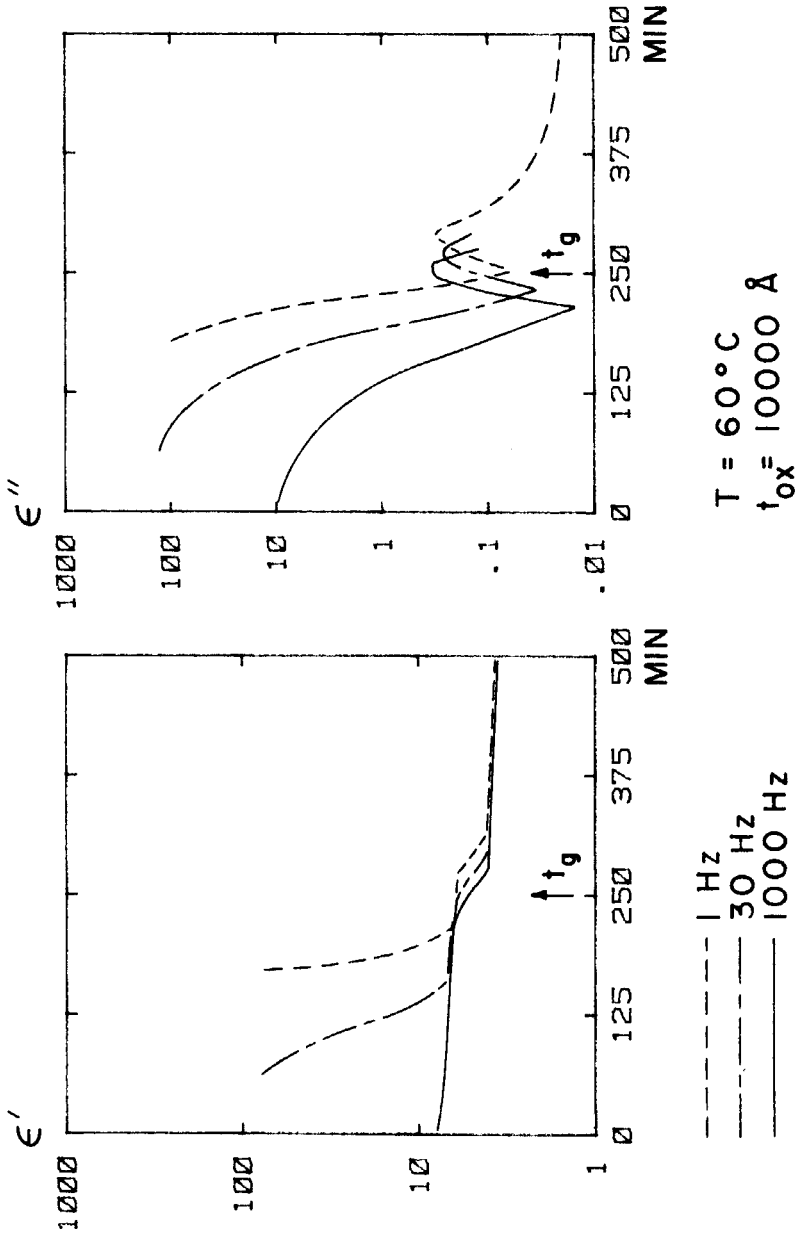


FIGURE 6 Time dependence of ϵ' and ϵ'' for DGEBA-MPDA cured at 60°C.

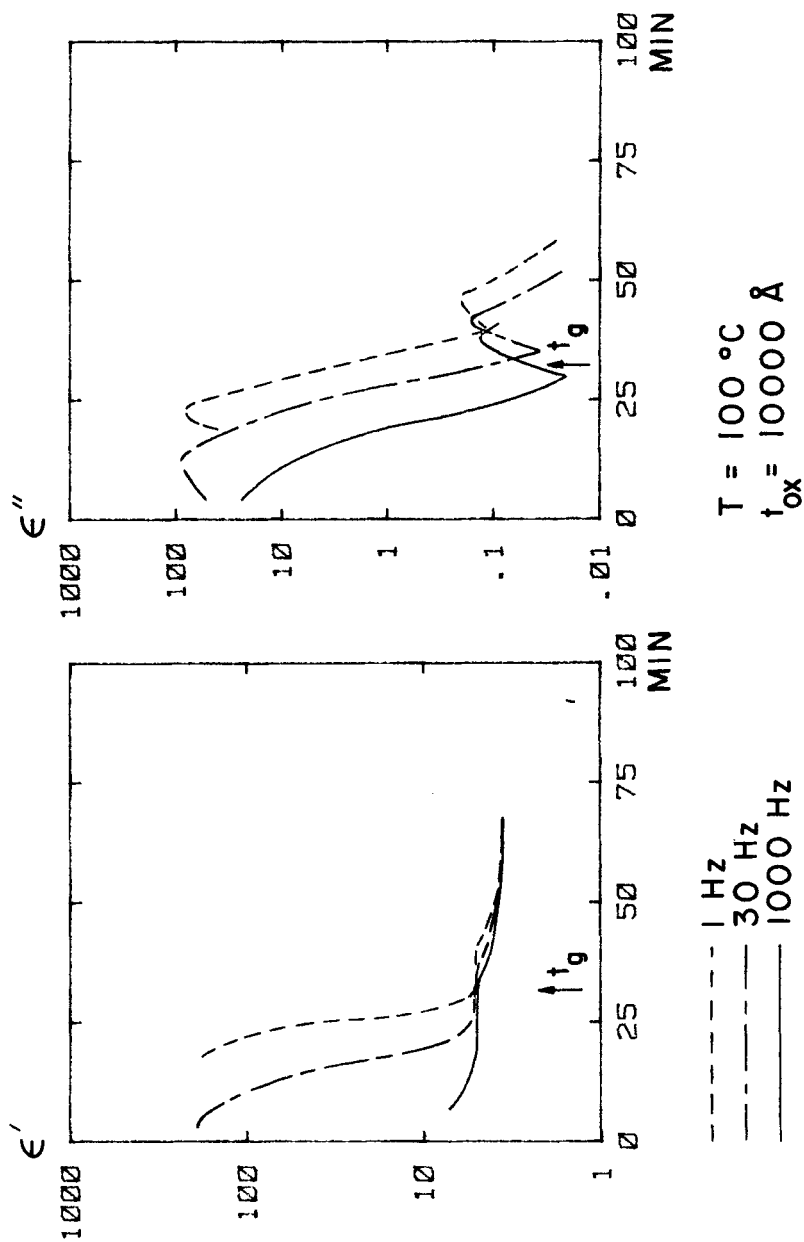


FIGURE 7. Time dependence of ϵ' and ϵ'' for DGEBA-MPDA cured at 100°C .

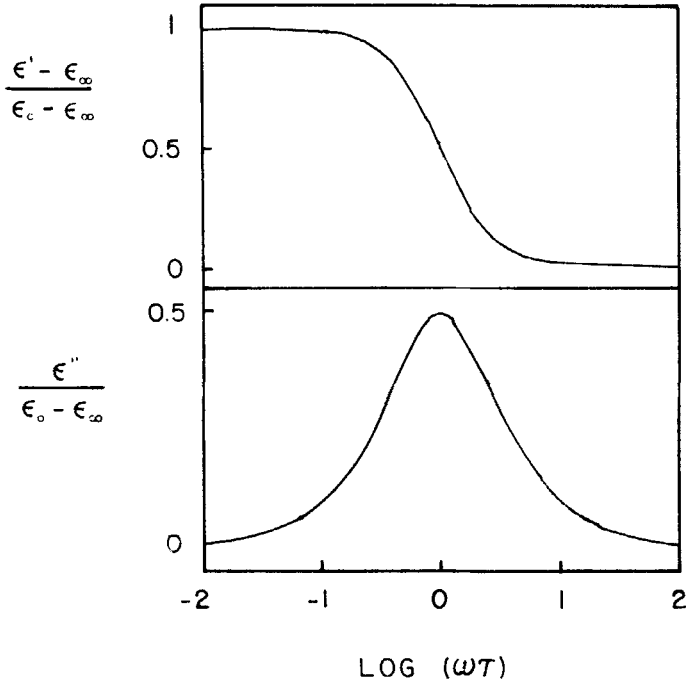


FIGURE 8 Dependence of ϵ' and ϵ'' on the $\omega\tau$ product for an ideal Debye relaxation.

permittivity is large, and the loss is low. Near $\omega\tau = 1$, ϵ' decreases and ϵ'' has a peak. For large $\omega\tau$, the permittivity is low and the loss is low. The effect of a constant bulk conductivity is to add a term to ϵ'' equal to the conductivity divided by the frequency. However, if the conductivity mechanism is itself a hindered process, with its own relaxation time, such a conductivity gives rise both to a modified ϵ'' and to a term in ϵ' which has the same form as for the Debye model. In the discussion to follow, we shall concentrate on the apparent Debye-like behavior of ϵ' and ϵ'' observed in this particular system, while for the experiments reported in the following section, we shall note the added presence of an apparent bulk conductivity contribution to ϵ'' early in cure. In neither case can we prove whether the observed Debye-like behavior is due to the hindered dipole rotation or to the hindered conduction mechanism, particularly for the pre-gelation behavior where the conductivity might be expected to be large.

Turning now to the data, and with the Debye model in mind, one can see that Figures 6 and 7 show two Debye-like relaxations: a large relaxation prior to gelation, and a smaller relaxation after gelation. The frequency dependence

demonstrates that the 1 Hz measurement is more sensitive to these relaxations than higher frequencies. Increased frequency or increased extent of cure make it more difficult for the dipoles to respond to the alternating electric field.

The pre-gelation data from all six experiments (three temperatures, two device geometries) were fitted to the ideal Debye model, and the time- and temperature-dependent dielectric relaxation time was extracted, as shown in Figure 9. For any one device, the agreement between the relaxation times determined from different frequencies at the same elapsed cure time was within 20%, whereas the agreement between the relaxation times determined from the devices with different oxide thicknesses at the same cure temperature was within 50%. Since the relaxation time changes by many orders of magnitude during cure, this degree of agreement is already very good. However, the results indicate that further refinements of the calibration may be required.

The time dependence of the pre-gelation relaxation time resembles the time dependence of the viscosity of thermosetting systems. For example, the slope of a log viscosity *versus* time plot breaks to a much steeper value as cure proceeds, which is attributed to chain entanglement among the branched polymers formed early in cure.⁸ In addition, at the start of cure, the higher temperature sample has a lower viscosity, but cures faster, so its viscosity *versus* time curve will cross the corresponding curve for a lower temperature. The data of Figure 9 show both these features. To illustrate the excellent correspondence between our relaxation-time data and the viscosity data reported by Kamal,⁹ Figure 10 shows an Arrhenius plot of the time to reach 8 sec relaxation time and Kamal's time to reach 400 poise viscosity. The points fall on a single line characterized by an activation energy of 11.5 Kcal/mole, indicating that the same process is responsible for the behavior of both the viscosity and the pre-gelation relaxation time.

B. PGE diluent in DGEBA-DDS

Phenyl glycidyl ether (PGE) is a monofunctional epoxide which can react with an amine functionality, reducing the ability of the system to form crosslinks. We have examined the effects of various amounts of PGE in DGEBA cured with diaminodiphenyl sulfone (DDS). DDS is tetrafunctional, but the effect of adding PGE diluent can be viewed as reducing the effective functionality of the amine. At 33 phr, the effective amine functionality becomes 3, and at 100 phr, the functionality becomes 2, at which point the system tends to form linear polymer rather than a crosslinked continuous network.

Figures 11 and 12 show ϵ' and ϵ'' , respectively, *versus* cure time at 140°C for each of four frequencies (1, 10, 100 and 1000 Hz) for various amounts of diluent. Measurements were also made at 100 phr, with results almost identical to the 80 phr data. The data in the figures at high loss factor have been

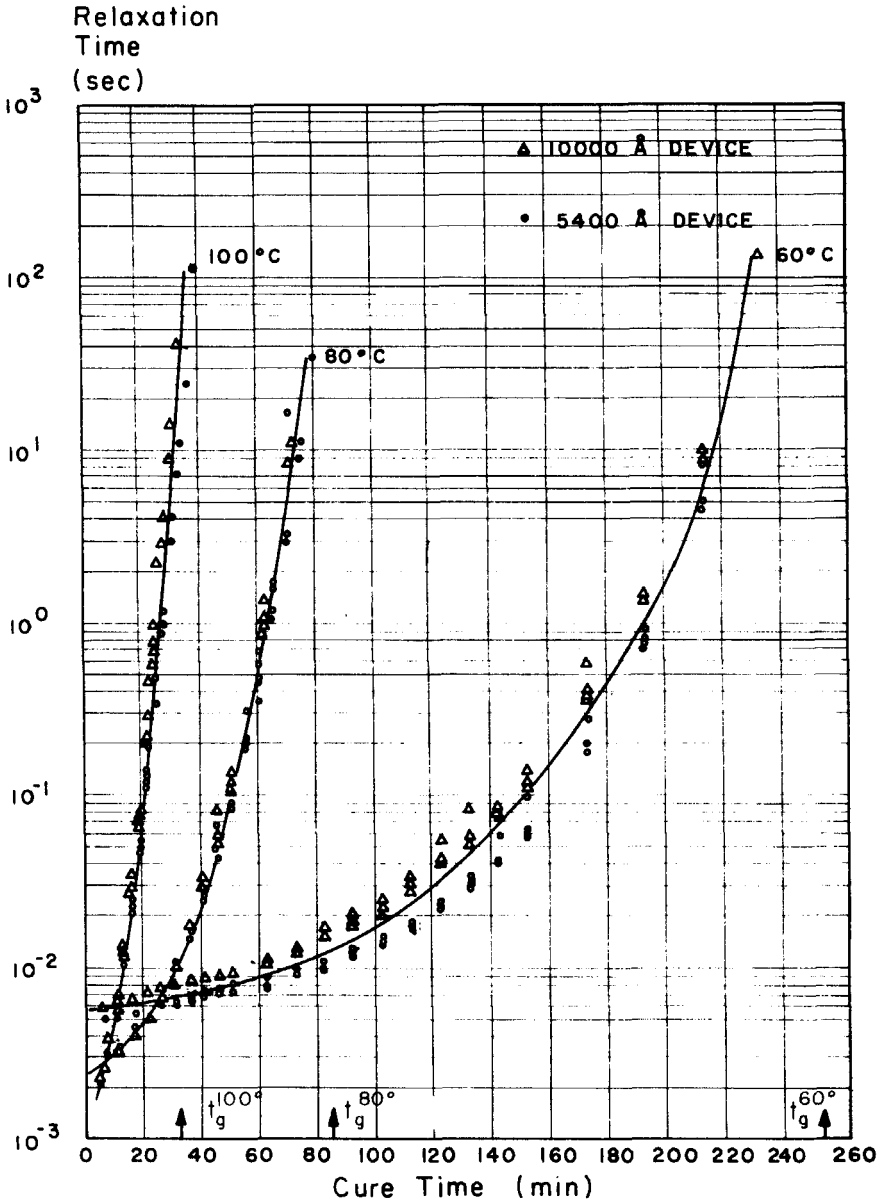


FIGURE 9 Time- and temperature-dependence of the dielectric relaxation time of DGEBA-MPDA prior to gelation.

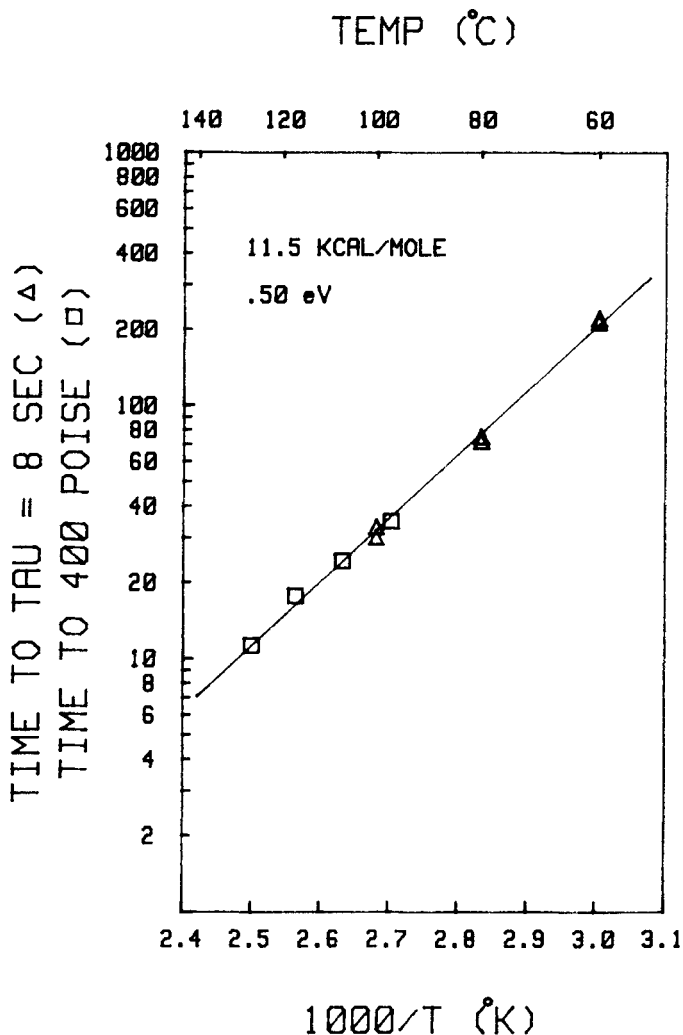


FIGURE 10 Arrhenius plot showing correlation between dielectric relaxation time and viscosity (Ref. 9).

manually smoothed to improve visibility. The raw data showed considerable noise above ϵ' values of 30, consistent with the calibration difficulties described earlier.

Referring first to Fig. 11, the post-gelation relaxation, at least for 0, 20, and 40 phr, resembles the results presented for the DGEBA-MPDA system. The pre-gelation relaxation observed for the DGEBA-MPDA system (Fig. 6 and

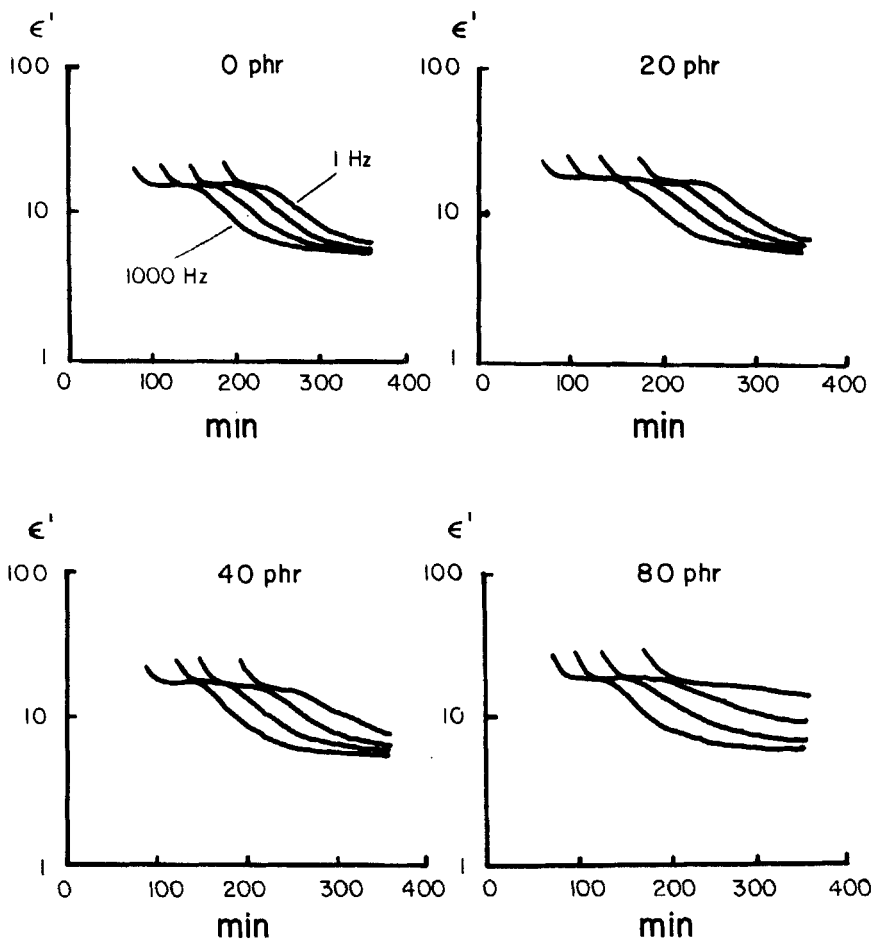


FIGURE 11 Permittivity ϵ' versus cure time at 1, 10, 100, and 1000 Hz for 0, 20, 40, and 80 phr PGE in DGEBA-DDS. Cure is at 140°C.

7), and expected at 90 min for this system based on the data of Babayevsky and Gillham,¹⁰ is not seen in Figure 11 because the relatively high bulk conductivities which occur at low cure times result in data that are beyond the present calibration capability. (The effect of a bulk conductivity is to add to ϵ'' a term equal to the conductivity divided by the frequency.) The conductivity decreases with cure time, but is still large enough to wash out the post-gelation loss peaks in Figure 12, except at 1000 Hz.

The most striking feature of the data is the similarity of the general shapes of the data for all diluent levels, excepting only the marked slowing of the

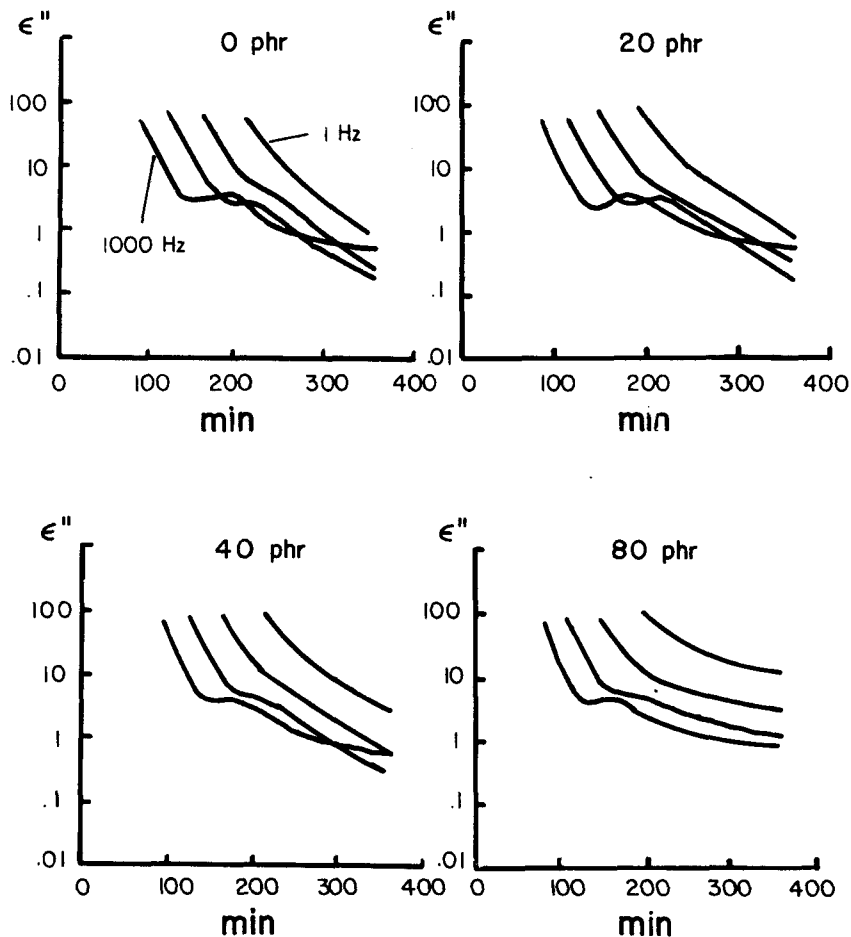


FIGURE 12 Loss factor ϵ'' corresponding to the conditions of Figure 11.

apparent cure rate with increasing amounts of diluent. In the case of 80 phr, the data show that the cure reaction has almost ceased at 360 min yet the ϵ' values at low frequencies have not decreased nearly as much as those ϵ' values of less diluted samples for corresponding times. This is consistent with the presence of diluent. That is, with diluent present, fewer crosslinks are formed, and the reaction ceases with a molecular network that is similar to what a partially cured non-diluted sample would exhibit if quenched during cure. This suggests that the glass transition temperatures of the samples should show a steady decrease with increasing amounts of diluent, and a post-cure ramped temperature experiment was carried out to examine this possibility.

Figures 13 and 14 show the ϵ' and ϵ'' data at 1 Hz for a set of samples first cured at 140°C for six hours, then cooled to room temperature, then subjected to a temperature ramp at 1 deg/min up to 150°C. Referring first to Figure 13, note the clear 1 Hz dielectric relaxation between 90 and 120°C for the 40 phr sample. This relaxation goes between ϵ' values of 5 and 14, and corresponds to what would be expected for the glass transition. Note also that at 80 phr, the corresponding relaxation is completed by 85°C, while for 20 phr, it is just beginning at 125°C. For the undiluted specimen, only the faintest onset of this relaxation is evident, even at 150°C, which is 10 degrees above the cure temperature.

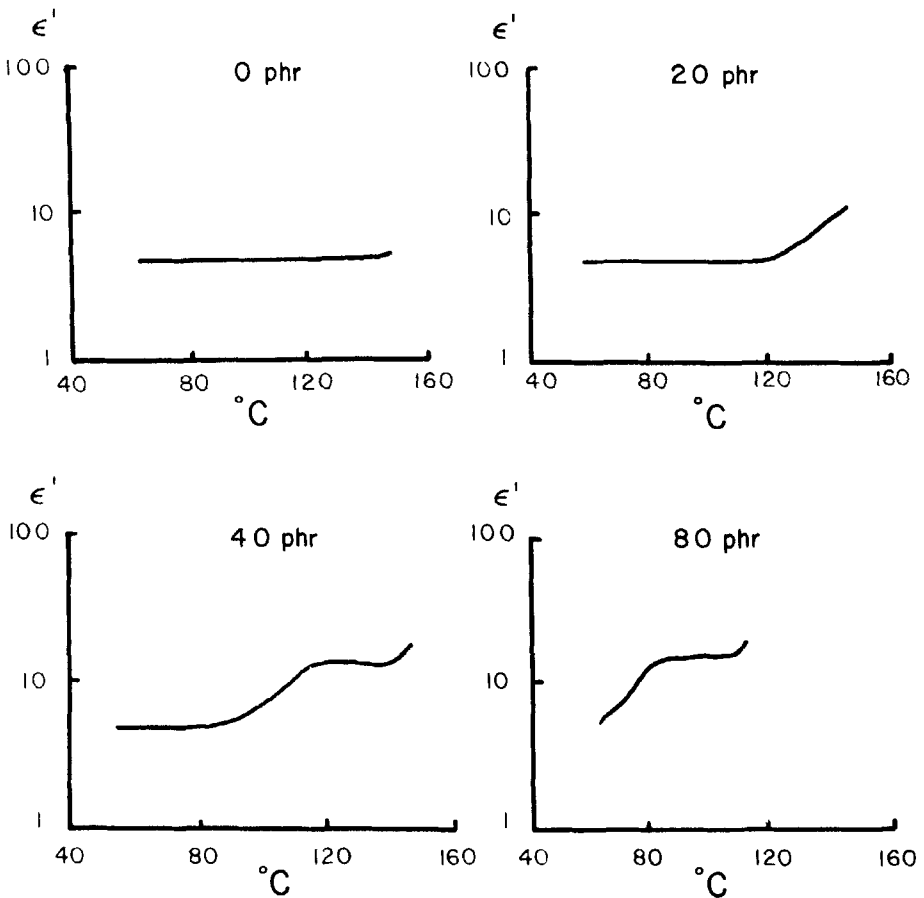


FIGURE 13 Post-cure behavior of ϵ' behavior at 1 Hz for DGEBA-DDS diluted with PGE. Heating rate is 1°C/min.

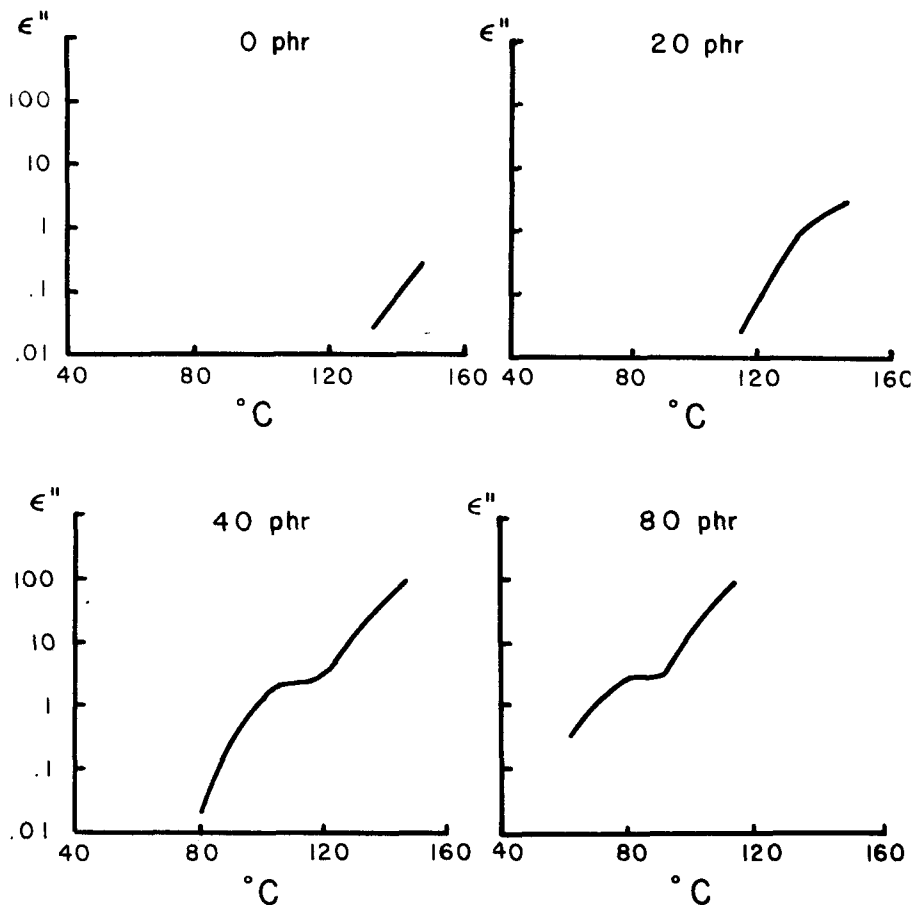


FIGURE 14 Loss factor data corresponding to Figure 13.

The ϵ'' post-cure data of Figure 14 correspond to what would be expected from the ϵ' data, provided a thermally activated conductivity term is added to ϵ'' . The initial increase in ϵ'' with temperature (Figure 14) result from dipole relaxations and agrees with what would be expected from the corresponding ϵ' relaxations (Figure 13). After the plateau in ϵ'' (the peak of the dipole loss) the thermally activated conductivity takes over causing a continued increase in ϵ'' with temperature. For the undiluted specimen, only slight evidence of the dipole relaxation is evident at 150°C.

The large sensitivity of the post-cure ϵ'' data to diluent concentration led us to perform additional experiments with 5 and 10 phr. The ϵ'' data for post-cure

temperature ramps are shown in Figure 15. Note that as little as 5 phr diluent produces observable changes in the ϵ'' value at 1 Hz. Note further that even with 10 phr diluent, the 1 Hz dielectric relaxation peak associated with the glass transition has not yet appeared, even at 150°C for samples cured six hours at 140°C.

All of the post-cure data can be summarized by somewhat arbitrarily selecting the "1 Hz loss peak temperature" as indicative of the glass transition. Using the Debye model for interpretation of the ϵ' data, this temperature corresponds to the point at which $\epsilon' = 10$. The $\epsilon' = 10$ temperature is plotted against diluent concentration in Figure 16. If this were a true plot of glass transition, one would expect the zero diluent case to have a point at 140°C, the

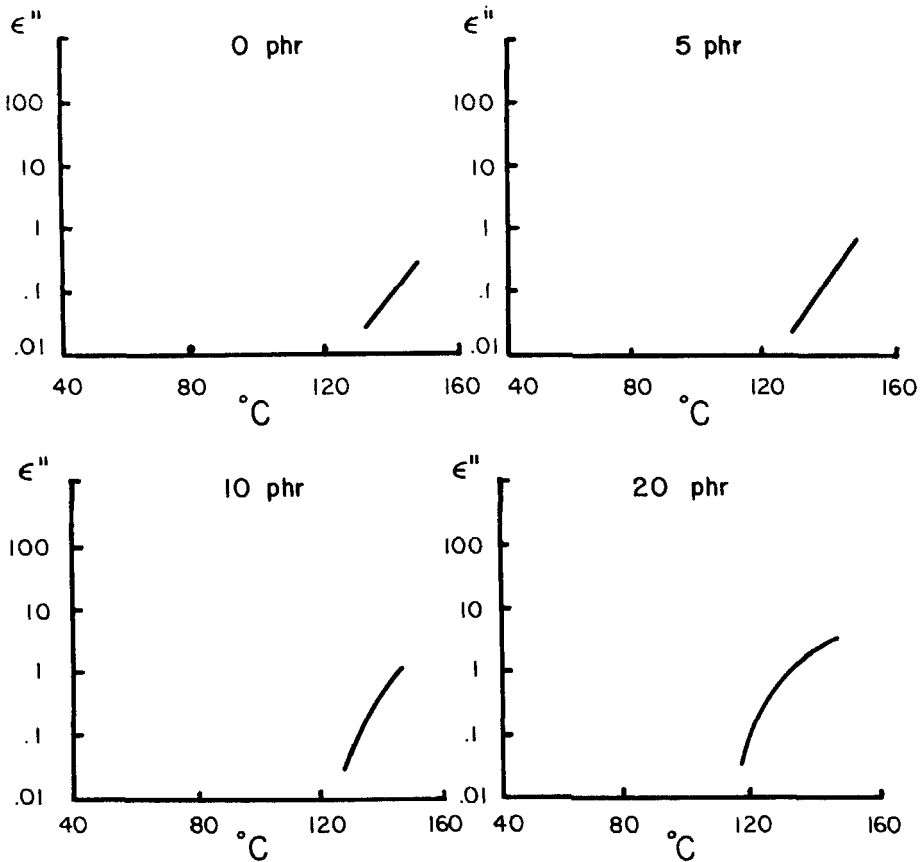


FIGURE 15 Loss factor data at 0, 5, 10, and 20 phr PGE in DGEBA-DDS measured at 1 Hz. Heating rate is 1°/min.

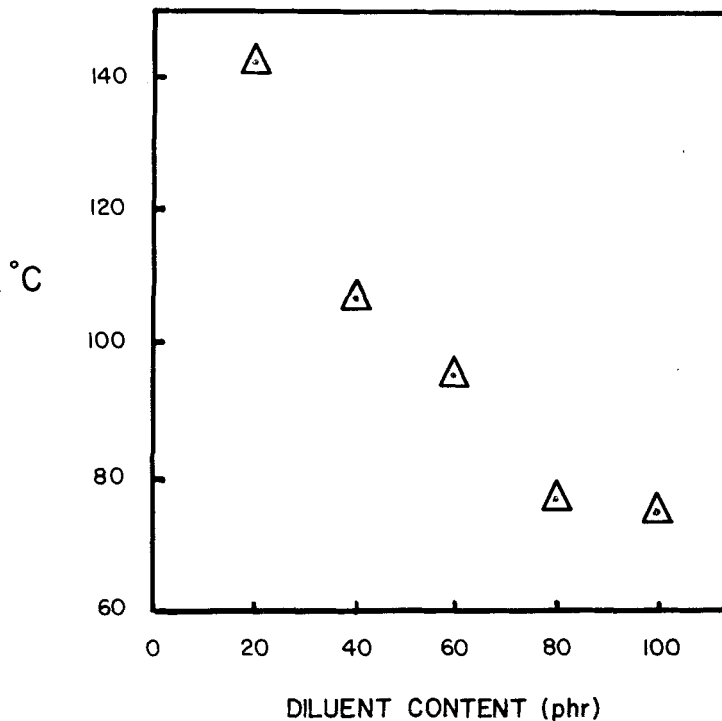


FIGURE 16 Effect of PGE concentration on 1 Hz relaxation temperature.

cure temperature, and the diluted samples to have progressively lower glass transition temperatures.¹¹ In our case, even the 20 phr sample has not gone through its loss peak at 140°C. However, the general behavior of the data with diluent concentration is reasonable. The conclusion from these results is that in spite of the fact that 1 Hz is a very low frequency at which to make dielectric measurements, it is still not low enough to be considered “near zero”. If one raises the undiluted specimen to the temperature at which it was cured, internal dipole orientations at 1 Hz are still effectively quenched. One must raise the temperature well above 140°C before a 1 Hz measurement will show a loss peak. In our case, even with 20 phr, the loss peak at 1 Hz occurs above the cure temperature.

CONCLUSIONS

This paper has demonstrated the use of Microdielectrometry for the study of curing in two epoxy-amine systems. A major conclusion is that for studies of

the networks formed during cure, there is a significant advantage in being able to extend the low-frequency limit of the experiment as far as possible. Indeed, with the diluent example, it is seen that even 1 Hz, which is already well below the lowest frequency available with conventional dielectric instrumentation, is still "too high" to make accurate glass transition temperature determinations. Furthermore, our results clearly demonstrate the value of being able to make measurements at multiple frequencies in real time. For example, the frequency dependence of ϵ' and ϵ'' at any instant can be analyzed in terms of models of dielectric relaxation, such as the viscosity in the case of pre-gelation data.

An important direction for future work, in addition to further exploration of the dielectric properties of networks formed with diluent, is to extend the measurement technique to even lower frequencies. Work is presently under way on a Fourier transform spectroscopy equivalent of Microdielectrometry, with which the low frequency limit should be easily extendable to 0.1 Hz or below.

Acknowledgements

This work was sponsored in part by the Office of Naval Research. The authors wish to thank Dr. L. H. Peebles, Jr., of ONR for his encouragement and for his welcome participation in technical discussions related to this program. Devices used in this work were fabricated in the M.I.T. Microelectronics Laboratory, a Central Facility of the Center for Materials Science and Engineering, which is sponsored in part by the National Science Foundation under Contract DMR-78-24185. Resins and curing agents used in these experiments were provided by Dr. N. Schneider of the Army Materials and Mechanics Research Center, Watertown, MA, U.S.A. Some of the equipment in the Microdielectrometry apparatus was purchased under NSF Contract ENG-7717219.

References

1. N. F. Sheppard, Jr., *et al.*, "Microdielectrometry: A New Method for In-Situ Cure Monitoring", Proc. 26th SAMPE Symposium, Los Angeles, CA, **26**, 65-76 (1981).
2. S. D. Senturia, *et al.*, "Microdielectrometry", Proc. A Critical Review: Techniques for the Characterization of Composite Materials, Cambridge MA, June 1981, in press.
3. N. F. Sheppard, Jr., *et al.*, "Microdielectrometry", Proc. Materials Research Soc., Boston MA, Nov. 1981, Sensors and Actuators, in press.
4. S. L. Garverick and S. D. Senturia, *IEEE Trans. Elec. Dev.* **ED-29**, 90-94 (1982).
5. H. L. Lee, S.M. Thesis, Massachusetts Institute of Technology, 1982, unpublished.
6. The results reported here have been previously published in Refs. 2 and 3. They are included here to illustrate the relaxation time approach to interpreting such data.
7. S. Sourer and M. R. Kamal, *Thermochimica Acta* **14**, 41 (1976).
8. F. G. Musatti and C. W. Macosko, *Polymer Eng. Sci.* **13**, 236 (1973).
9. M. R. Kamal, S. Sourer and M. Ryan, "Integrated Thermo-Rheological Analysis of the Cure of Thermosets", Soc. Plast. Eng. 31st Annual Tech. Conf., Montreal, May 1973, p. 187.
10. P. G. Babayevsky and J. K. Gillham, *J. Appl. Polym. Sci.* **17**, 2067-2088 (1973).
11. J. K. Gillham, *Polymer. Eng. Sci.* **19**, 676 (1979).